

**Amendments to the Specification**

Please replace the paragraph starting on page 1, line 3 with the following rewritten paragraph:

This a continuation of Serial No. 09/747,094, filed December 22, 2000, now U.S. Patent No. 6,660,030 ~~6,660,202~~, which is a continuation-in-part of Serial No. 09/525,778, filed March 15, 2000, now U.S. Patent No. 6,500,202, which is a continuation-in-part of Serial No. 09/251,363, filed February 17, 1999, now U.S. Patent No. 6,197,049, which is a continuation-in-part of Serial No. 09/210,280, filed December 11, 1998, now U.S. Patent No. 6,187,036, the disclosures of each of which are incorporated by their entireties herein by reference.

Please replace the paragraph starting on page 18, line 14 with the following rewritten paragraph:

Referring to FIGS. 13 and 14, there is illustrated a fragmentary side elevational view of an enhanced flexibility embodiment of the deployment catheter of the present invention. In this embodiment, the distal component ~~134~~ 135 of the central tubular core 132 comprises a flexible wall such as a braided polyimide tubing. In one embodiment, the polyimide tubing has an inside diameter of about 0.059" and an outside diameter of about 0.071". An internal braid is made from 0.0015" stainless steel 304 wire at a pic count of about 50 braids per inch, such as may be obtained from Phelps Dodge (GA) or H.V. Technologies (GA). The use of flexible tubing such as spiral cut layers or woven or braided tubing in place of conventional stainless steel or other metal hypotubing increases the lateral flexibility of the assembled device, which facilitates the placement and deployment steps.

Please replace the paragraph starting on page 18, line 25 with the following rewritten paragraph:

However, introduction of a flexible hypotube ~~134~~ 135 creates a flex point in the catheter at about the junction 131 between the distal end 129 of outer sheath 128 and the proximal end of the outer tubular housing 138. To prevent kinking at the junction 131, a reinforcement structure 161 is preferably provided within the catheter, spanning the junction 131. In the illustrated embodiment, the reinforcement structure 161 is carried by the tubular extension 160 of intermediate tube 130. The reinforcement structure 161 is in the form of a tubular element such

as a stainless steel hypotube. The illustrated hypotube has a length within the range of from about 40 mm to about 60 mm, a wall thickness within the range of from about 0.002" to about 0.005" and is secured immovably to the tubular extension 160. Any of a variety of other reinforcement structures 161 can also be used, such as spiral cut or woven or braided layers, polymeric tubing and the like, depending upon the desired performance characteristics. By positioning the reinforcement structure 161 at about the axial location of the junction 131, the flexibility characteristics of the catheter can be optimized, while permitting a highly flexible hypotube ~~434~~ 135.

Please replace the paragraph starting on page 19, line 17 with the following rewritten paragraph:

The braided polyimide hypotube ~~434~~ 135, or other braided or woven reinforced tubular element can be secured to the enlarged diameter proximal component 134 of tubular core 132 (see FIG. 14) in any of a variety of ways. In the illustrated embodiment, a threaded insert 163 is adhesively bonded to the polyimide hypotube component ~~434~~ 135 of the tubular core 132 using a flexible epoxy such as 310 T manufactured by Epotech (MASS.) or other adhesives known in the art.

Please replace the paragraph starting on page 19, line 31 with the following rewritten paragraph:

In this embodiment, the proximal end 165 of ipsilateral tubular sheath 162 is tapered such as by necking down the outside diameter of the ipsilateral tubular sheath 162 for bonding to the tubular extension 160. This creates a generally conical space within the end of the tubular sheath 162, which can potentially collapse and cause binding upon distal advance of the outer sheath 128. Thus, a plug ~~463~~ 177 having a generally conical shape may be provided to fill the proximal end 165 of the ipsilateral tubular sheath 162, thereby presenting a surface ~~467~~ 175 for facing the graft (not illustrated). The plug ~~463~~ 177 may be manufactured in any of a variety of ways, such as by injection molding or machining, or by introducing a curable or otherwise hardenable agent into the proximal end 165 and curing it in place to provide a surface ~~467~~ 175.

Please replace the paragraph starting on page 20, line 9 with the following rewritten paragraph:

Another optional feature of the deployment catheter is a spacer 173 ~~174~~. In the embodiment illustrated in FIG. 10, for example, it can be seen that the outside diameter of the ipsilateral tubular sheath 162 tapers down to approximately the inside diameter of the tubular extension 160, which is considerably smaller than the outside diameter of the intermediate tube 130. This low diameter space between the ipsilateral tubular sheath 162 and intermediate tube 130 creates an opportunity for the distal end of the outer sheath 128 to become engaged (snagged) with the proximal end 165 of sheath 162 as the outer sheath 128 is advanced distally along the deployment device. This may occur, for example, after the outer sheath 128 has been proximally retracted to release the contralateral graft, and thereafter distally advanced to support the ipsilateral graft during deployment of the contralateral graft.